

# Using a Kinetic Model of Human Gait in Personal Navigation Systems

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**Driven to Discover<sup>SM</sup>**

# Personal Navigation: Why?

- Personal navigation systems: Navigators that can be carried or worn by individuals
  - Primarily, generate a position solution.
  - Can provide velocity and attitude solution as well.
- Significant current interest in personal navigation systems for applications such as:
  - Location-based computing (e.g., cell phones, laptops, etc)
  - Assisted Living
  - Guidance for Visually impaired.
  - First responders (fire fighters, EMTs)
  - **Post surgery monitoring of patients**
  - **Law enforcement & Military** (e.g., urban navigation, cave navigation, etc.)
  - **Biometrics: Identify a person by gait.**



**Guidance for  
the Visually  
Impaired**



**First Responder  
Navigation**



# Personal Navigation Solutions

- Most current personal navigation solutions are GPS-based.
  - Work well outdoors and away from urban canyons
  - Work poorly (or not at all) indoors
- Solutions based on other **position fixing** techniques are being explored.
  - Wi-Fi, Ultra Wide Band (UWB), Electro Optical/Infrared Cameras
  - Advantage: Position errors do not grow with time
  - Disadvantage: Infrastructure intensive
- **Dead reckoning** solutions are self contained and address some of the issues associated with position fixing systems
  - Step counting (pedometer) , shoe-mounted inertial navigation (NavShoe™ from Intersense), body-mounted inertial navigation.
  - Advantages: Self contained.
  - Disadvantages: Errors grow with time (“random walk”)



# Inertial Navigation Systems (INS)

- Inertial Navigation Systems (INS): Self-contained navigators equipped with sensors continuously measuring acceleration ( $\mathbf{a}$ ) and rotation/rotation rate ( $\omega$ ), from which velocity ( $\mathbf{v}$ ), position ( $\mathbf{p}$ ) and attitude/orientation ( $\mathbf{C}_n^b$ ) are computed.

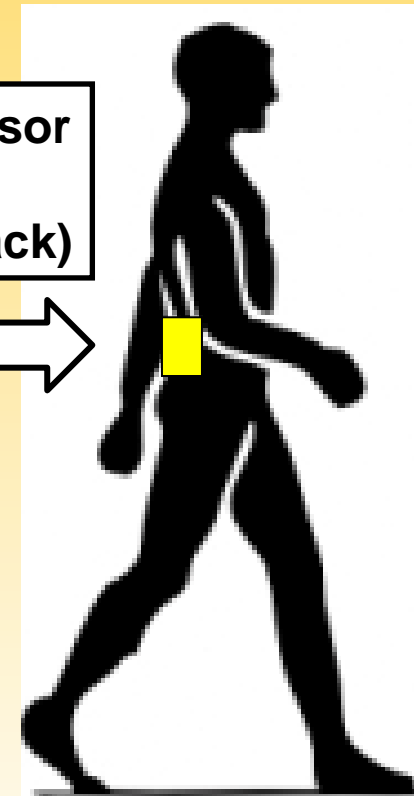
$$\mathbf{v} = \mathbf{v}_0 + \int_0^t \mathbf{a} \, dt$$

**Velocity Equation**

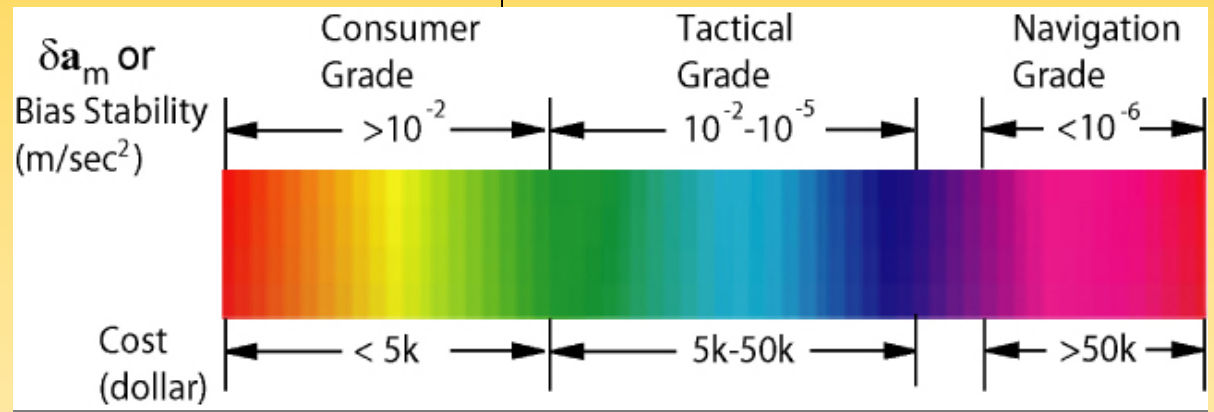
$$\mathbf{p} = \mathbf{p}_0 + \int_0^t \mathbf{v} \, dt = \mathbf{p}_0 + \int_0^t \int_0^\tau \mathbf{a} \, d\tau \, dt$$

**Position Equation**

Inertial Sensor Suite  
(small of back)



# INS Quality Spectrum vs Error



$$\mathbf{a}_m = \mathbf{a} + \delta\mathbf{a}$$

$$\hat{\mathbf{v}} = \mathbf{v}_0 + \int_0^t \mathbf{a}_m dt$$

$$= \mathbf{v}_0 + \int_0^t \mathbf{a} dt + \int_0^t \delta\mathbf{a} dt$$

$$= \mathbf{v} + \delta\mathbf{v}(t)$$



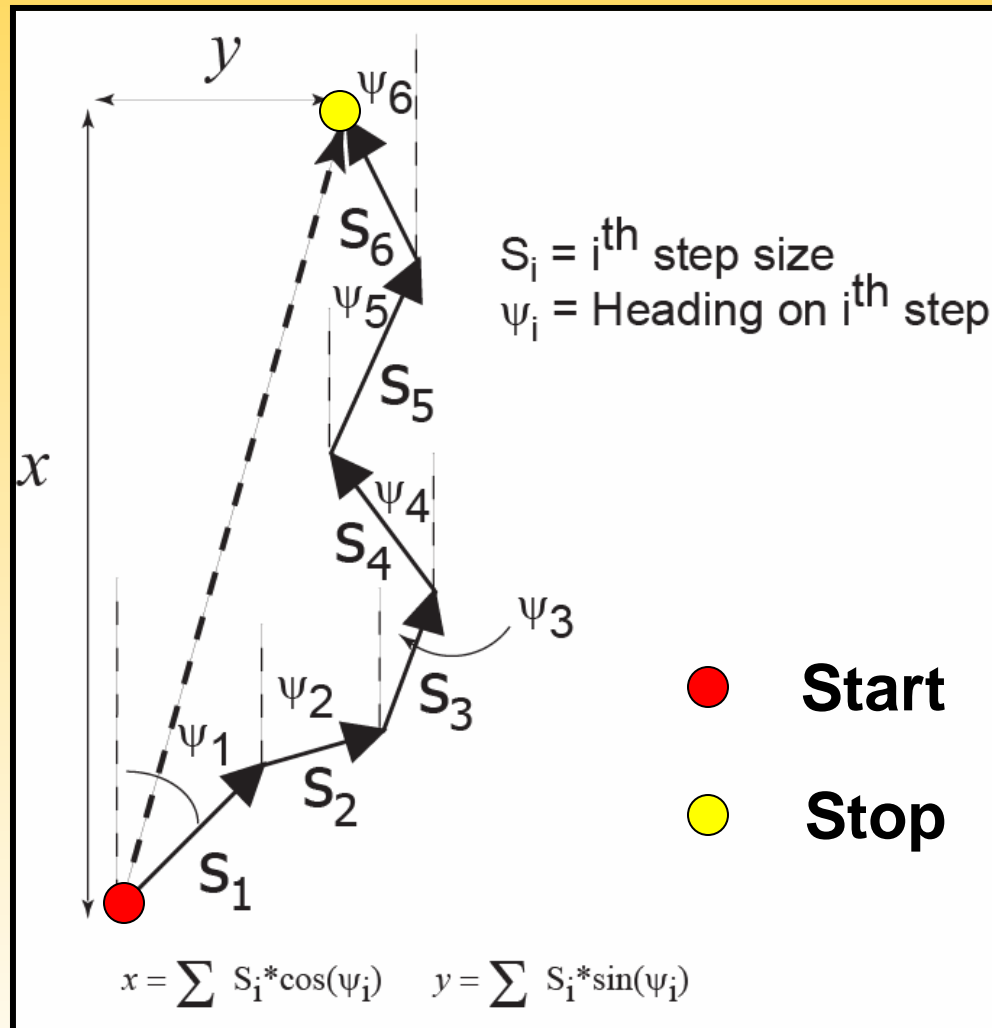
# Bounding INS Drift with ZUPs



- Can use zero velocity updates (ZUPs) to bound position error drift
  - $\mathbf{V}$  at the end of each step is zero
- **Advantage:** Position error ( $\Delta p$ ) is becomes a linear function of time of travel ( $T$ ) as opposed to a quadratic or cubic growth seen by traditional INS.
- **Problem:** Direction of travel or heading can be of poor quality if not aided by information from another source.



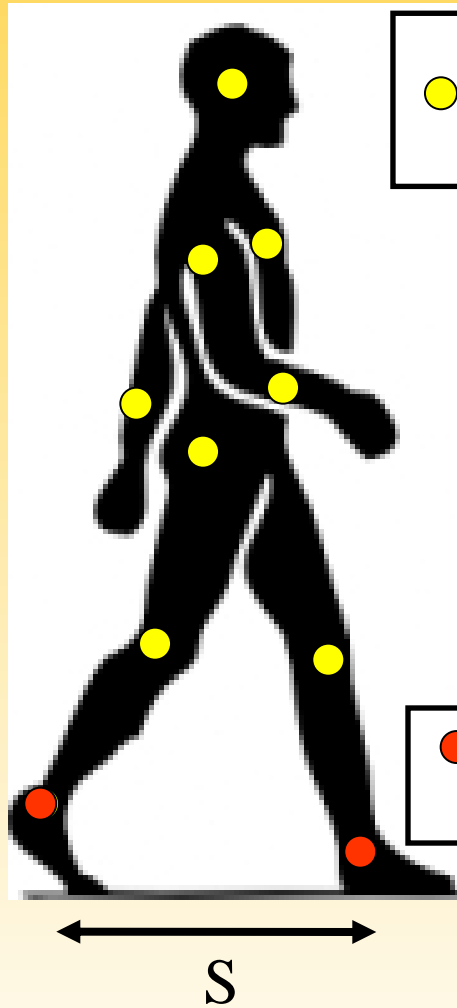
# Step Counting (Pedometer)



- Need a way to measure
  - The distance traveled during each step (**not a simple problem**)
  - The direction of travel (heading) during each step.
- Steps can be counted by using a sensor like an accelerometer.
- Direction of travel can be determined using a compass (magnetometer triad).



# Motion Model: A Virtual Sensor?



● Potential Site  
For measuring  
Kinematic States

- Can knowledge of human motion be used as a **sensor or constraint** in personal navigation systems?
- What are the important parameters to characterize human motion (from a navigation point of view) ?

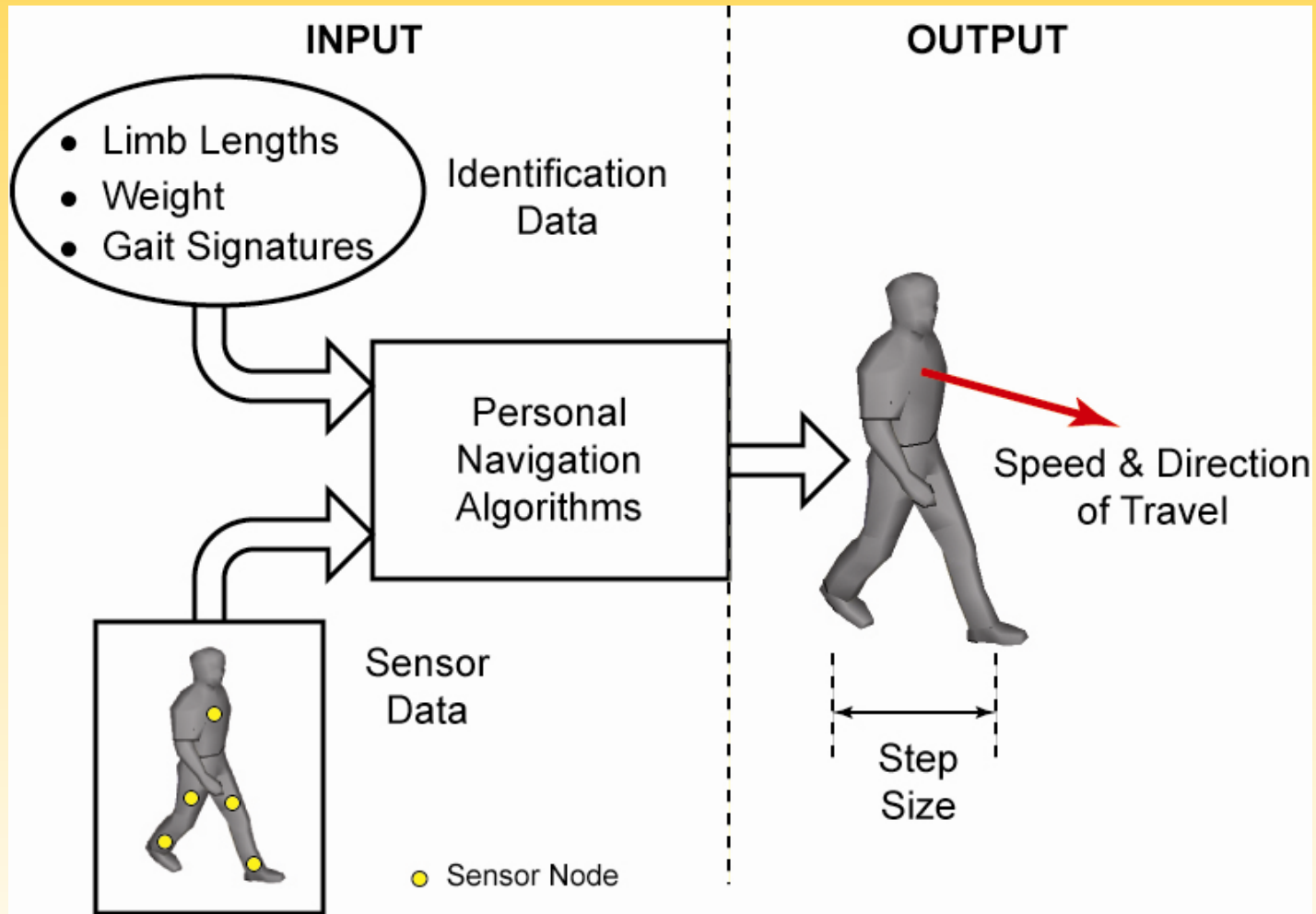
● Linear  
Acceleration

**Yes.** This talk is about using such models to estimate step size or  $S$ .

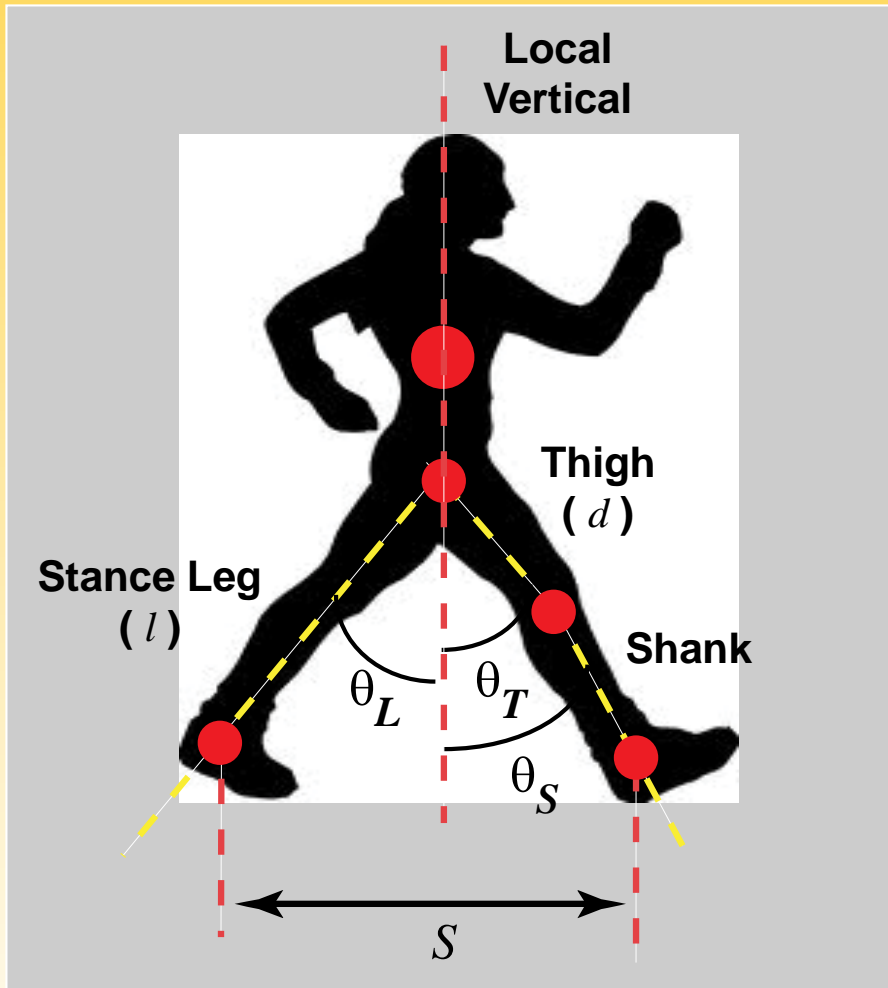




# Proposed Approach



# Step Size & Gait Kinematics

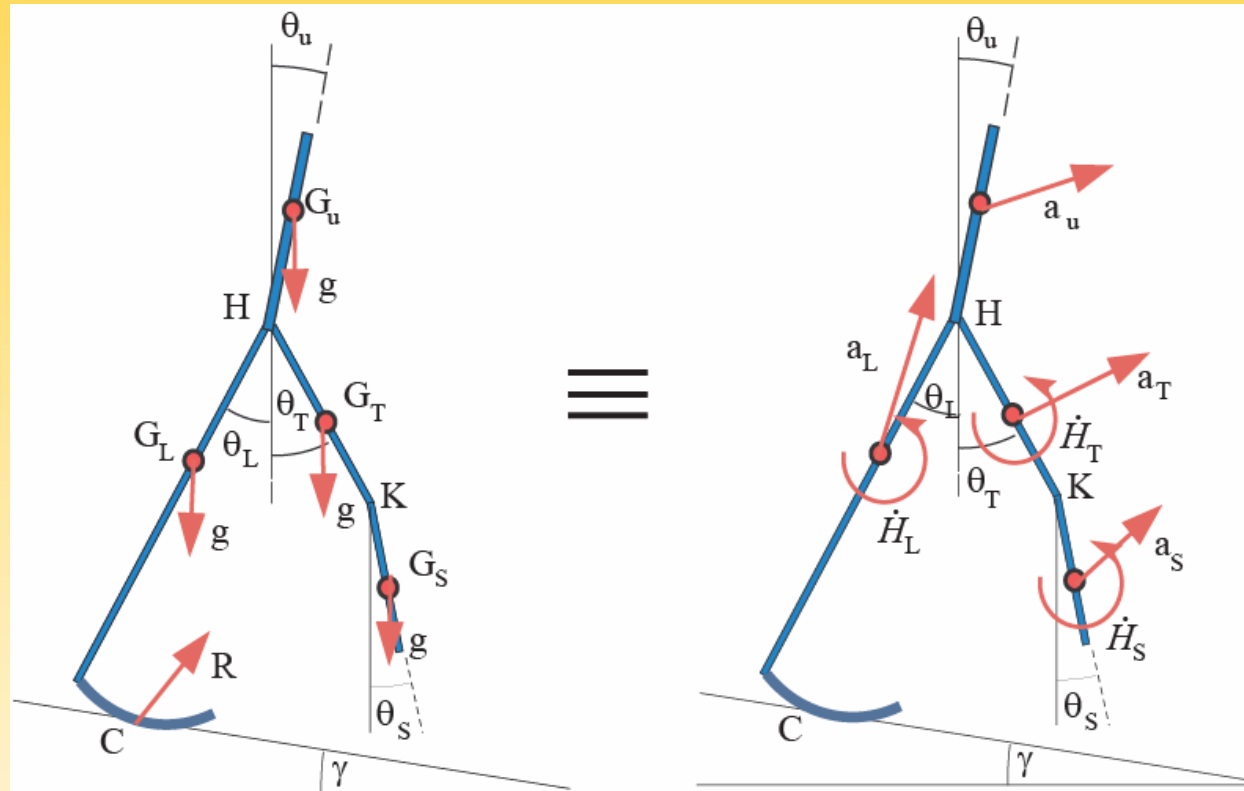


- Let us assume that we are dealing with a person walking in a straight line.
  - No heading change
- Let us also assume we are dealing with normal walking
  - No running, skipping, shuffling, etc.
- Then a time history of limb angles can be used to estimate step size ( $S$ ).

$$S = l \sin \theta_L + d \sin \theta_T + (l - d) \sin \theta_S$$



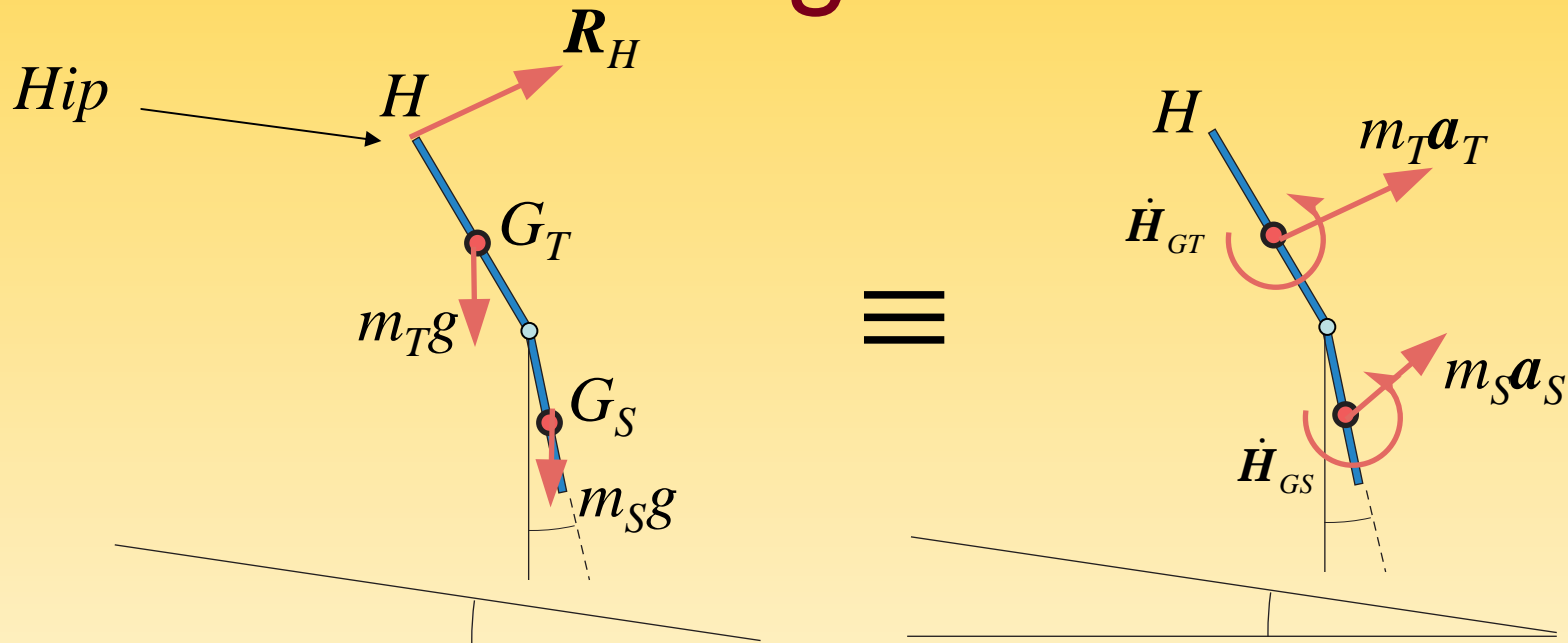
# The Passive Walker



- The passive walker is an idealization of human gait.
- It assumes the motive force is gravity and ignores muscular inputs.



# Thigh & Shank Free Body Diagrams

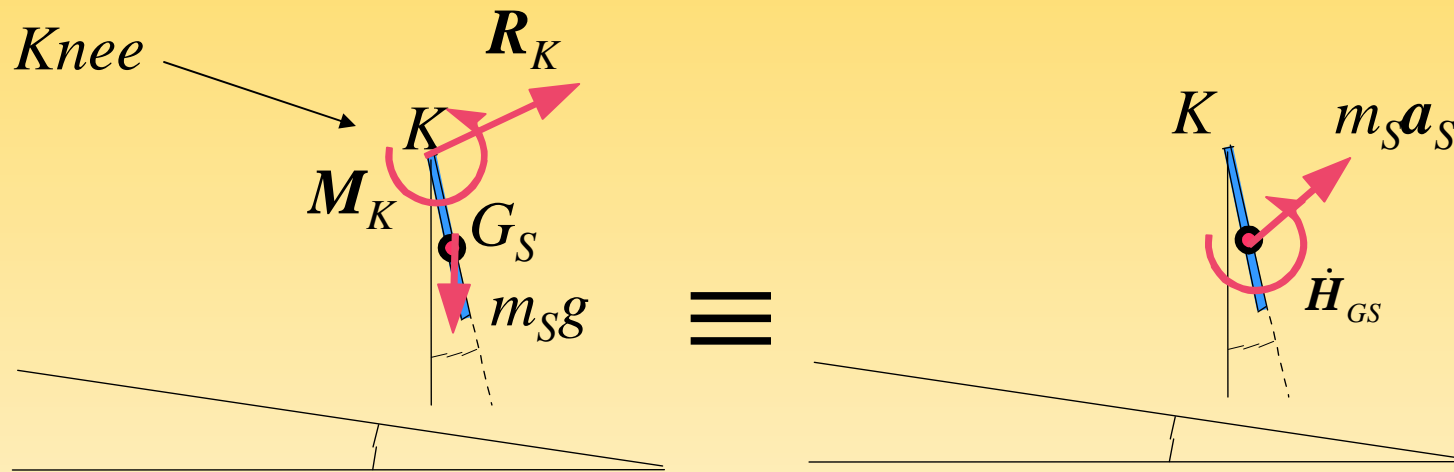


$$\sum M_H : \quad \mathbf{r}_{HG_T} \times m_T \mathbf{g}_T + \mathbf{r}_{HG_S} \times m_S \mathbf{g}_S =$$

$$\bar{\mathbf{r}}_{HG_T} \times m_T \mathbf{a}_T + \bar{\mathbf{r}}_{HG_S} \times m_S \mathbf{a}_S + \dot{\mathbf{H}}_{GT} + \dot{\mathbf{H}}_{GS}$$



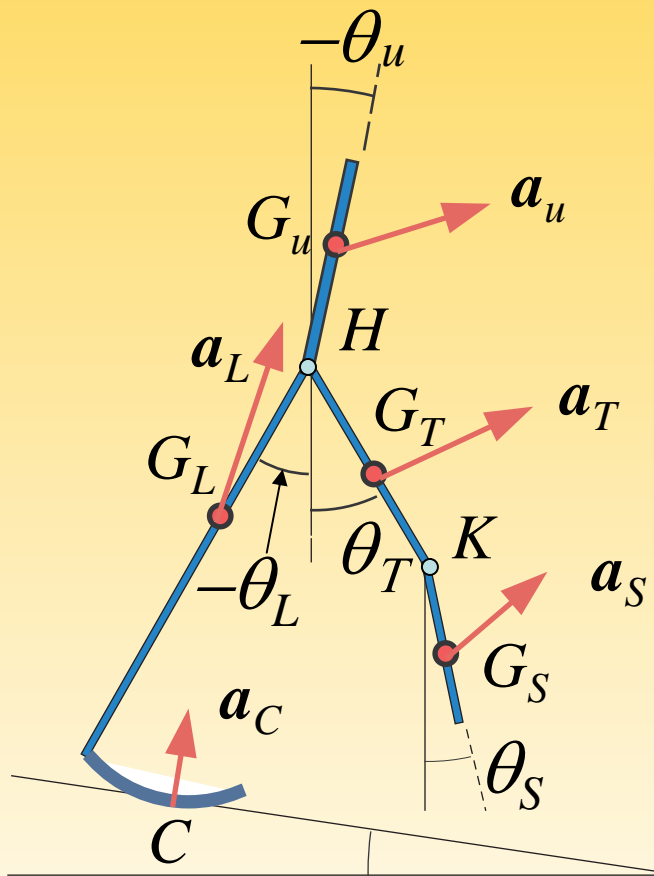
# Shank Free Body Diagram



$$\sum \mathbf{M}_K : \mathbf{r}_{KG_S} \times m_S \mathbf{g}_S + \mathbf{M}_K = \bar{\mathbf{r}}_{CG_S} \times m_S \mathbf{a}_S + \dot{\mathbf{H}}_{GS}$$



# Passive Walker Kinematics



$$\omega_L = \dot{\theta}_L \mathbf{k} \quad \omega_S = \dot{\theta}_S \mathbf{k}$$

$$\omega_T = \dot{\theta}_T \mathbf{k}$$

$$\dot{\theta}_u = 0$$

Ignoring  
Torso Sway

$$\mathbf{a}_{G_L} = \mathbf{a}_C + \dot{\omega}_L \times \mathbf{r}_{CG_L} + \omega_L \times \omega_L \times \mathbf{r}_{CG_L}$$

$$\mathbf{a}_H = \mathbf{a}_C + \dot{\omega}_L \times \mathbf{r}_{CH} + \omega_L \times \omega_L \times \mathbf{r}_{CH}$$

$$\mathbf{a}_u = \mathbf{a}_H$$

$$\mathbf{a}_{G_T} = \mathbf{a}_H + \dot{\omega}_T \times \mathbf{r}_{HG_T} + \omega_T \times \omega_T \times \mathbf{r}_{HG_T}$$

$$\mathbf{a}_K = \mathbf{a}_H + \dot{\omega}_T \times \mathbf{r}_{HK} + \omega_T \times \omega_T \times \mathbf{r}_{HK}$$

$$\mathbf{a}_{G_S} = \mathbf{a}_K + \dot{\omega}_S \times \mathbf{r}_{KS} + \omega_S \times \omega_S \times \mathbf{r}_{KS}$$



# Passive Walker Equations

- The passive walker equations from the previous slides can be recast into a the following form:

$$\mathbf{M}\ddot{\boldsymbol{\theta}} = \mathbf{A}(\dot{\boldsymbol{\theta}}, \boldsymbol{\theta})$$

$$\ddot{\boldsymbol{\theta}} = \mathbf{M}^{-1}\mathbf{A}(\dot{\boldsymbol{\theta}}, \boldsymbol{\theta})$$

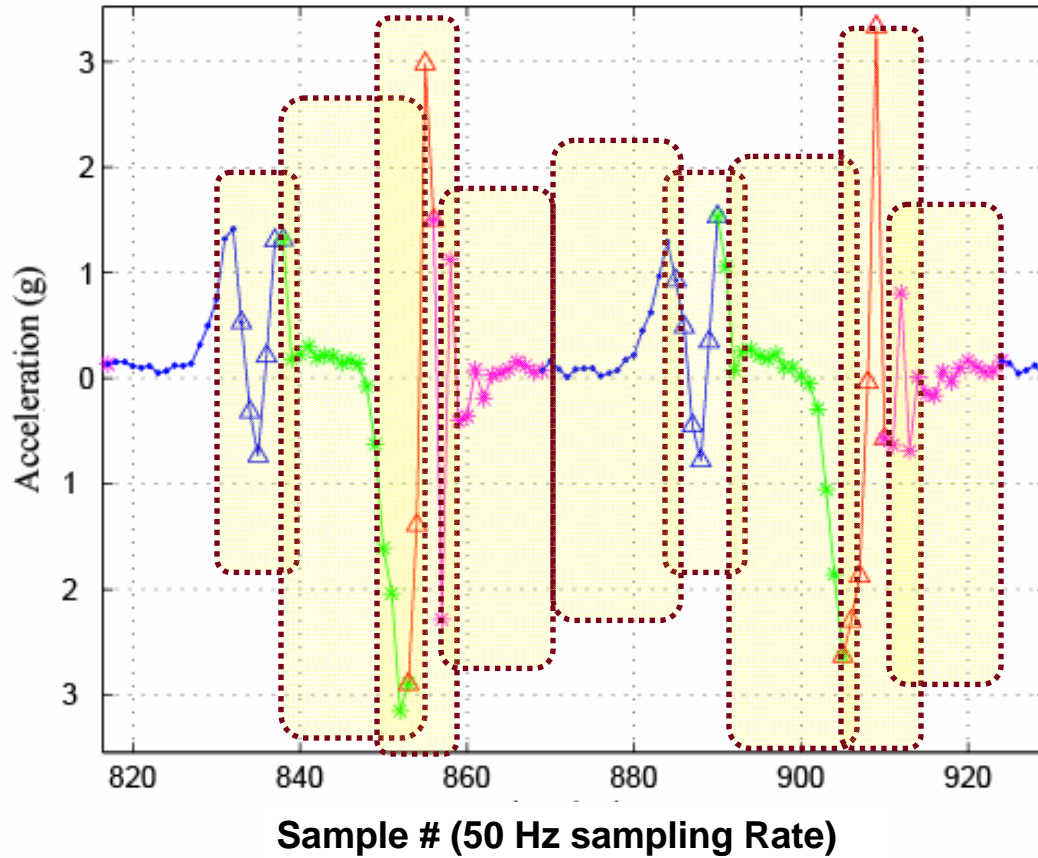
$$\boldsymbol{\theta} = [\theta_L \quad \theta_T \quad \theta_S]^T$$

- This form, in turn, can be recast in a non-linear, state-space form which looks like:

$$\dot{\mathbf{x}} = \begin{bmatrix} \dot{\theta}_L \\ \dot{\omega}_L \\ \dot{\theta}_T \\ \dot{\omega}_T \\ \dot{\theta}_S \\ \dot{\omega}_S \end{bmatrix} = \mathbf{f}(\mathbf{x}) = \begin{bmatrix} \omega_L \\ G_1(\boldsymbol{\theta}, \dot{\boldsymbol{\theta}}) \\ \omega_T \\ G_2(\boldsymbol{\theta}, \dot{\boldsymbol{\theta}}) \\ \omega_S \\ G_3(\boldsymbol{\theta}, \dot{\boldsymbol{\theta}}) \end{bmatrix}$$



# Gait-Cycle: Ankle Acceleration



1. Pick Up and Go

2. Swing Phase

3. Impact

4. Weight Transfer

5. Stance Phase





# Modified Passive Walker

- We can use the acceleration at the ankle ( $\mathbf{a}$ ), input to the passive walker equations (an indirect measure of muscular torques)

$$\ddot{S} = \ddot{S}(\mathbf{a}) = \frac{d}{dt} (l \sin \theta_L + d \sin \theta_T + (l - d) \sin \theta_S)$$

- We also augment the state vector with an additional set of states to account for applied torques at the knee and ankle of the swing leg (assume quadratic over the step).

$$M_k = p_{k_0} + p_{k_1} t + p_{k_2} t^2$$

$$M_c = p_{c_0} + p_{c_1} t + p_{c_2} t^2$$

- The unknowns in these moment equations are the coefficients of the quadratic moment model.



# Solving Modified PW Equations

- Given the initial conditions on angular velocities, we can use the accelerometer outputs to integrate the modified passive walker equations.
- What are the initial conditions?
  - For angles: we assume initial conditions for the current step are the angles at the end of the last step.
  - Angular rates: We solve for them.
- Basically, we solve an optimization problem
  - Unknowns are the initial conditions for angular rates and the moment coefficients
  - Solution is based on a set of terminal constraints.
    - Heuristic as well as physics based constraints
    - For example, the height of the foot at the end of the step should be zero.

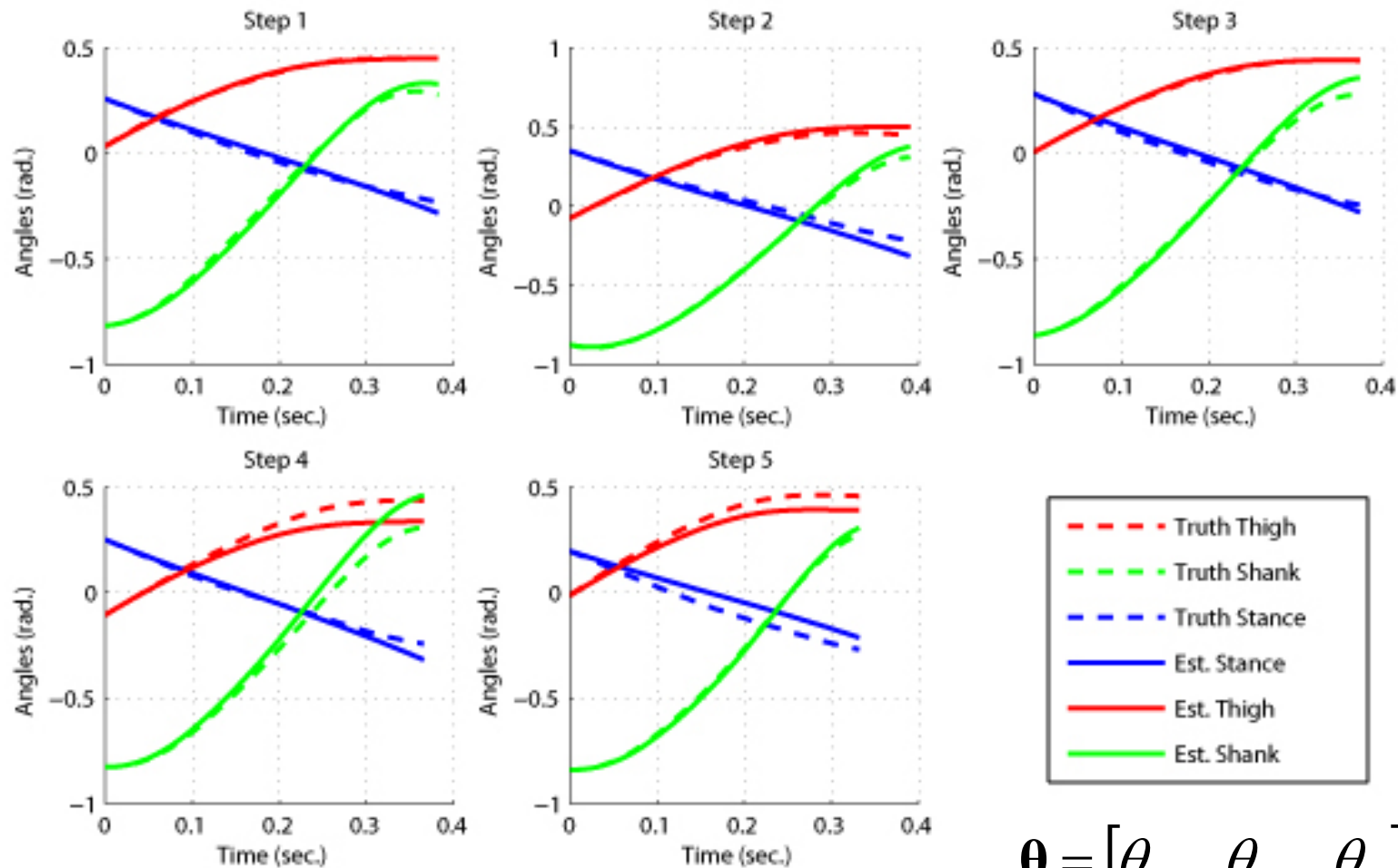


# Experimental Results

- One way we tested out results is by using data collected at the James R. Gage Center for Gait and Motion Analysis (Gillette Children's Hospital in St. Paul).
- Data collected from subjects walking in straight line and their motion was tracked using a Vicon™ motion tracking systems.
- Data was used to generate time history of limb kinematic states (position, velocity, accelerations, angular rates).
- Data was replayed in modified passive walker equations developed for this work.



# Five Step Time History for $\theta$



$$\theta = [\theta_L \quad \theta_T \quad \theta_S]^T$$

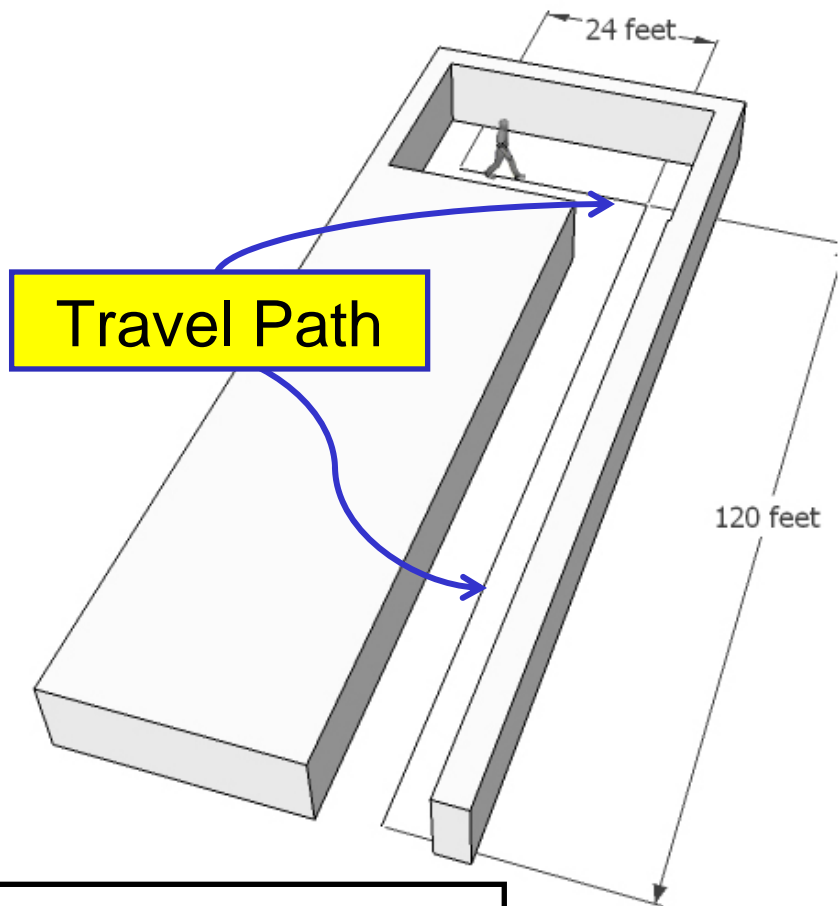


# Step Counting Experiments

- Performed a series of experiments to assess the viability of estimating step size or stride length in-situ indoors.
- Subject (C. Matthews) had an IMU strapped to each ankle
  - MIDG II INS/GPS unit
  - Tile count/size provided truth reference while CPU time on the MIDG is used as the time base.



# Basement Navigation Experiment



**Akerman Hall Basement  
(Concrete Building)**



**MIDG II  
INS/GPS Unit**



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# In-Situ Step Size Estimates

- Figures show that the model does a reasonable job of estimating the two varying step sizes (24" = 61 cm and 36" = 91.4 cm)
- Note that in this case, a measurement from a single accelerometer is used to augment the state vector:



# Distance Traveled (Integrated Step Size)



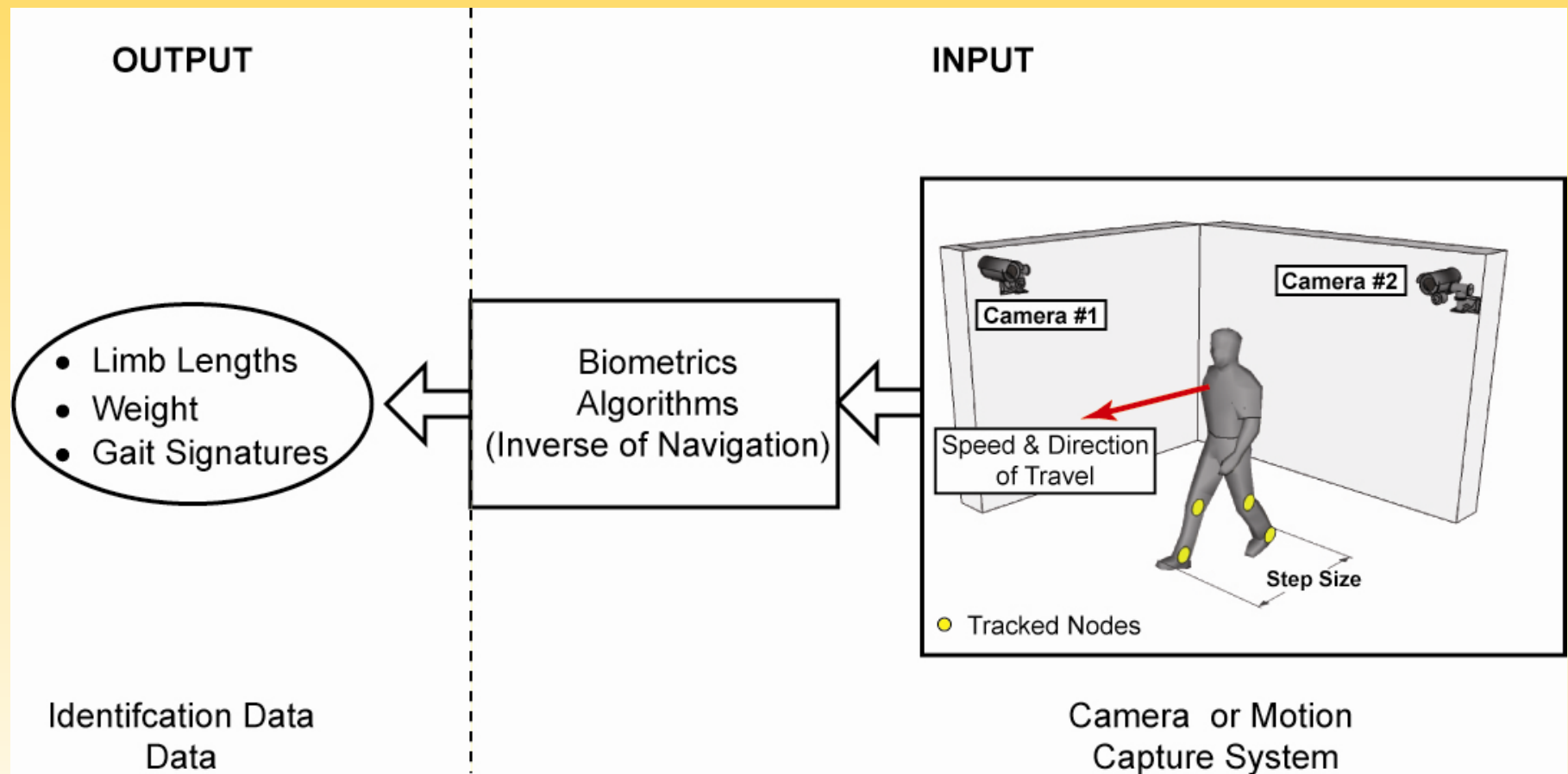


# Summary & Future Work

- Developed an approach for in-situ step size estimation (*c.f.*, C. J. Matthews, et al, “In-Situ Stride Length Estimation Using a Kinetic Model of Human Gait,” ION-GNSS 2010)
- Based on a kinetic model of gait and driven by a single acceleration measurement.
  - Adequate for “normal” step sizes
  - Cannot deal with turns or non-normal gait.
- On going work attempts to address turning motion as well as other non-normal gait patterns.
- Another thrust is to examine how gait characteristics can be used as means of identifying of persons.



# Model Identification or Biometrics



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